

REVIEWS

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Acrylic Resin Cytotoxicity for Denture Base – Literature Review

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A – research concept and design; B – collection and/or assembly of data; C – data analysis and interpretation; D – writing the article; E – critical revision of the article; F – final approval of article; G – other

Abstract

Acrylic resin is a widely used material in clinical practice, and a satisfactory biocompatibility is essential. When the resin polymerization reaction is incomplete, residual monomers are released into the oral cavity. The aim of this study was to evaluate, through a literature review, the cytotoxicity caused by the denture base acrylic resin used, and its components. The selection of published studies was performed on the Pubmed database from January 2008 to July 2013. The keywords used were: “cytotoxicity and acrylic resins”, “cytotoxicity and denture base resins” and “cytotoxicity and oral prosthesis”. Inclusion criteria were: *in vitro* studies and literature reviews published in English that evaluated the acrylic resin cytotoxicity for denture base and its components. Studies with no reference to the search strategy were excluded. A total of 182 articles were found. Among these, only 13 were included for writing this review. The MTT test is the most common test used to evaluate acrylic resin cytotoxicity. Auto-polymerized resin is more cytotoxic than heat-polymerized resin because of its higher quantity of residual monomers which cause cell and tissue changes in the oral mucosa. However, more studies are necessary for the development of biocompatible materials (Adv Clin Exp Med 2015, 24, 4, 679–686).

Key words: acrylic resins, cytotoxicity tests, biocompatibility testing.

Acrylic resin (PMMA – Polymethylmethacrylate) is a widely used material in dentistry [1–4]. Due to its utilization in temporary crowns, denture fabrication, reline and repair, orthodontic appliances, splints for orthognathic surgery and others, this material should have the appropriate physical, chemical and biological properties [2, 3, 5–7].

Acrylic resin polymerization is crucial for the optimization of the material’s physical and biological properties because it allows the conversion of monomers into polymers [8]. Residual monomers and toxic chemical products such as formaldehyde, methacrylic acid, benzoic acid, dibutyl phthalate, phenyl benzoate, phenyl salicylate and, especially, MMA (methyl methacrylate), are produced on the denture base when the polymerization process is incomplete [2, 3, 5, 6, 8–11]. These monomers, released in the aqueous environment

of the oral cavity, are present even when polymerization is performed according to the manufacturer’s recommendations [6, 9–11].

The cytotoxicity of acrylic resins and their components is evaluated by *in vitro* studies [1–3, 5–8, 10–13]. The cytotoxicity test is performed with extracts of acrylic resin specimens, which indirectly measure the material’s biocompatibility, by their action on cell cultures [2, 6, 9, 14].

This test can also determine the toxic concentrations of tested material and its consequences on cell morphology and growth, degree of cellular damage and enzymatic activities in a particular cell type. In other words, this test defines the material’s biological behavior and its components [2, 6, 9].

The methods for cytotoxicity analysis are described and regulated by ISO-standard 10993-5 [1, 8, 11]. Bural et al. [8] reported that this classi-

fication is based on the cytotoxicity degree of the tested material as follows: non-cytotoxicity (cell proliferation greater than 75%), slight cytotoxicity (50–75% of cell proliferation), moderate cytotoxicity (25–50% of cell proliferation) and high cytotoxicity (cell proliferation less than 25%).

The purpose of this study was to (1) review the published studies regarding the cytotoxicity of acrylic resin for denture bases and its components, (2) identify tests used for cytotoxicity analysis and (3) different responses according to the acrylic resin polymerization methods.

Material and Methods

The published studies selection was performed on the Pubmed database from January 2008 to July 2013. The keywords used were: “cytotoxicity and acrylic resins”, “cytotoxicity and denture base resins” and “cytotoxicity and oral prosthesis”. Inclusion criteria were: *in vitro* studies and literature reviews published in English that evaluated the acrylic resin cytotoxicity for denture bases and its components. Studies with no reference to the search strategy were excluded. Two reviewers read the selected studies and their information was analyzed and discussed for writing this review.

Results and Discussion

A total of 182 articles were found and 19 studies were selected according to the search strategy (Table 1). Figure 1 presents the study flow chart.

Cytotoxicity Tests

Different methods are used for cytotoxicity analysis in the literature. Among them, the most common is the MTT test (3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium), which quantifies

the mitochondrial succinate dehydrogenase enzyme activity and measures the conversion of water-soluble tetrazolium salt in insoluble blue formazan by spectrophotometry. This test is an excellent marker of cell survival because it evaluates cellular respiratory activity [1, 2, 5, 9, 10, 12].

The flow cytometry technique can be performed to evaluate the cell viability and apoptosis [3, 6, 7]. In addition, a cell proliferation analysis can be executed using bromodeoxyuridine incorporation (BrdU) [1] or XTT assay (sodium 3'-[1-phenylaminocarbonyl]-3,4-tetrazolium]bis(4-methoxy-6-nitro)benzenesulphonic acid), which measure the reduction of XTT in soluble formazan product [8]. The gene expression is evaluated by the RT-PCR (reverse transcription-polymerase chain reaction) which analyzes the mRNA production for collagen and other proteins and enzymes [3, 4, 6]. Furthermore, a cell's DNA and RNA synthesis can be measured by ³H-thymidine and H-uridine assays, respectively [5, 9, 10].

However, these tests are rarely performed because of their high cost, advanced technology requirement and radioactive wastes [5, 10]. Enzyme-linked immunosorbent assay (ELISA) is an immunoenzyme method that allows detection of specific antibodies and is used for cytotoxicity analysis [10, 13]. The comet assay evaluates DNA damage (genotoxicity) [1]. Cellular lipid metabolism and cell morphology analysis are other methods for cytotoxicity evaluation [6, 9].

The *in vitro* test advantages, such as the MTT test, include the facility of implementation in different cell types, reproducibility, precise control of variables and cost-effectiveness [5, 8, 10]. However, this test does not completely represent the material cytotoxic properties in their clinical condition. Therefore, such results can not be extrapolated to the general population. The reason is that the oral mucosa, due to keratin and mucin layers, is more resistant to toxic substances than cell cultures [2, 6, 8, 10].

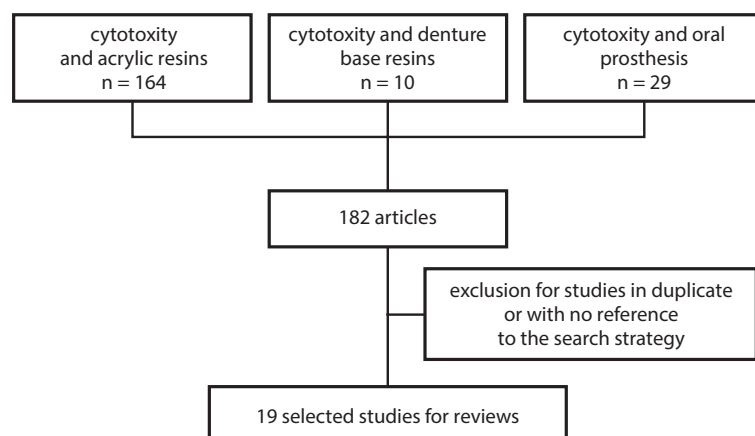


Fig. 1. Flow chart of selected publications for inclusion in the review

Table 1. Studies selected for the review according to the search strategy

Authors	Tested materials	Assays	Periods of analysis	Cell type	Results
Acosta-Torres et al. [1]	<ul style="list-style-type: none"> • Nature-Cryl – HR • PMMA • PMMA + AgNP 	<ul style="list-style-type: none"> • MTT • BrdU assay • Comet assay 	24 h, 72 h	<ul style="list-style-type: none"> • NIH-3T3 mouse embryonic fibroblast • Jurkat human lymphocyte cell line 	<ul style="list-style-type: none"> • non-cytotoxic materials • cell viability was present • these materials can be used to make biocompatible resins
Ata & Yavuzylmaz [2]	<ul style="list-style-type: none"> • AR – Meliodent • HR – Meliodent • POM 	<ul style="list-style-type: none"> • MTT 	1 h, 1 d, 3 d, 5 d, 7 d	L929 fibroblast cell line	<ul style="list-style-type: none"> • AR showed > cytotoxicity than HR after 1 d ($p < 0.05$) • POM showed > cytotoxicity after 3 d, 5 d, 7 d • the lower the incubation periods, the higher the cytotoxicity
Kojima et al. [3]	<ul style="list-style-type: none"> • DuraSeal (PMMA) – AR • R + NAC (PMMA) • polystyrene 	<ul style="list-style-type: none"> • flow cytometry • RT-PCR (type I COL and dentin sialoprotein) • cell density • SOD, intra-cellular glutathione and alkaline phosphatase activities 	24 h, 3 d, 5 d, 7 d, 10 d, 20 d	rat dental pulp cell	<ul style="list-style-type: none"> • necrosis after 24 h: 45% (AR) X 27% (R + NAC and Polystyrene) • AR was negative for alkaline phosphate activity after 5 d and 10 d • COL I and dentin sialoprotein genes were expressed in R + NAC culture and barely expressed in AR culture • AR decreased cell viability and odontoblast-like cell phenotype
Hattori et al. [4]	<ul style="list-style-type: none"> • MMA 	<ul style="list-style-type: none"> • RT-PCR (for <i>Gsta1</i> promoter) 	–	human hepatoma HepG2 cell	<ul style="list-style-type: none"> • MMA increased <i>Gsta1</i> transcription
Tay et al. [5]	<ul style="list-style-type: none"> • Lucitone 550 – HR • soft-liners: Ufi-Gel P – Silicon • Dentuflex – AR • Trusoft – AR • Dentusoft – Tissue conditioner ≠ water storage time after polymerization 	<ul style="list-style-type: none"> • ³H-thymidine incorporation assay 	–	L929 fibroblast cell line	<ul style="list-style-type: none"> • Trusoft showed slightly cytotoxic effect and Dentuflex showed moderated cytotoxic effect • Lucitone-550: slightly cytotoxic effect after 24 h and non-cytotoxic effect when stored in water for 48 h • thermal treatment did not reduce the cytotoxicity effect of the acrylic-based soft liners ($p > 0.05$)
Att et al. [6]	<ul style="list-style-type: none"> • Unifast II – AR • R + NAC 	<ul style="list-style-type: none"> • flow cytometry • RT-PCR (for type I and type III COL) • COL production • cell density 	2 d, 5 d	rat palatal fibroblast	<ul style="list-style-type: none"> • cell viability: 2% (AR) X 35% (R + NAC) • AR reduced the expression of COL I and III genes and its production in 3 times

Table 1. Studies selected for the review according to the search strategy – cont.

Authors	Tested materials	Assays	Periods of analysis	Cell type	Results
Yamada et al. [7]	<ul style="list-style-type: none"> • AR • R + NAC 	<ul style="list-style-type: none"> • flow cytometry 	24 h	Odontoblast-like cell	<ul style="list-style-type: none"> • cell viability: 20% (AR) X 45% (R+NAC) • AR showed a tendency for apoptosis, increased reactive oxygen species production and decreased intracellular glutathione level and cell viability and function
Bural et al. [8]	<ul style="list-style-type: none"> • Meliodent – HR ≠ polymerization cycles (≠ MMA_r) 	<ul style="list-style-type: none"> • XTT 	1 d, 2 d, 5 d, 7 d	L929 fibroblast cell line	<ul style="list-style-type: none"> • increase of MMA_r in eluates of specimens polymerized with cycle without terminal boiling • the lower the incubation periods, the higher the cytotoxicity • use of terminal boiling for at least 30 min and water storage of the denture bases for at least 1 to 2 d are recommended
Ebrahimi Saravi et al. [10]	<ul style="list-style-type: none"> • AR – Futura Gen • AR – GC Reline Hard • HR – Meliodent 	<ul style="list-style-type: none"> • MTT • ELISA 	1 h, 24 h, 1 week	L929 fibroblast cell line	<ul style="list-style-type: none"> • AR showed > cytotoxicity than HR either after 1 h or 24 h (p < 0.05) • the lower the incubation periods, the higher the cytotoxicity
Bural et al. [11]	<ul style="list-style-type: none"> • Meliodent Rapid Repair – AR ≠ post-polymerization heat-treatments 	<ul style="list-style-type: none"> • XTT 	1 d, 2 d, 5 d, 7 d	L929 fibroblast cell line	<ul style="list-style-type: none"> • MMA_r reduced cell proliferation after elution of 1 d, 2d, 5d • all groups presented slightly cytotoxic effect after 7 d • post-polymerization heat-treatment is recommended to reduce MMA_r
Regis et al. [12]	<ul style="list-style-type: none"> • MMA • MUPB 	<ul style="list-style-type: none"> • MTT 	48 h	L929 fibroblast cell line	<ul style="list-style-type: none"> • high concentrations of MMA (1 g/L) reduced cell viability (p < 0.05) • MUPB presented > cytotoxicity than MMA
Zheng et al. [13]	<ul style="list-style-type: none"> • HR • HR + MMT 	<ul style="list-style-type: none"> • MTT • ELISA 	2 d, 4 d, 7 d	Vero cell	<ul style="list-style-type: none"> • non-cytotoxic materials
Trubiani et al. [14]	<ul style="list-style-type: none"> • Tokuyama Rebase Fast II – AuR • Ivoclar Probond Cold – AuR • Goldpack Tooth Acrylic – AuR polished or unpolished 	<ul style="list-style-type: none"> • MTT • ELISA • Western blot assay 	24 h, 48 h, 72 h	human gingival fibroblast	<ul style="list-style-type: none"> • polishing procedure can reduce the cytotoxicity

Table 1. Studies selected for the review according to the search strategy – cont.

Authors	Tested materials	Assays	Periods of analysis	Cell type	Results
Trubiani et al. [14]	<ul style="list-style-type: none"> • Tokuyama Rebase Fast II – AuR • Ivoclar Probase Cold – AuR • Goldpack Tooth Acrylic – AuR polished or unpolished 	<ul style="list-style-type: none"> • MTT • ELISA • Western blot assay 	24 h, 48 h, 72 h	human gingival fibroblast	<ul style="list-style-type: none"> • polishing procedure can reduce the cytotoxicity
Kanie et al. [15]	<ul style="list-style-type: none"> • Soft-liners based on urethane acrylate oligomers: • UA-160TM • UV-3200B • UV-3500BA • UV-3700B 	<ul style="list-style-type: none"> • MTT 	7d	<ul style="list-style-type: none"> • human cervical carcinoma-derived cell • human gingival carcinoma-derived cell 	<ul style="list-style-type: none"> • high cell viability (over 95.2%)
Segeström et al. [16]	<ul style="list-style-type: none"> • Carbon-graphite fiber-reinforced polymers (based on MMA/PMMA) – HR 	<ul style="list-style-type: none"> • MTT 	24 h	L929 fibroblast cell line	<ul style="list-style-type: none"> • non-cytotoxic materials
Dawlee et al. [17]	<ul style="list-style-type: none"> • MMA + GMA with iodine 	<ul style="list-style-type: none"> • MTT 	24 h	L929 fibroblast cell line	<ul style="list-style-type: none"> • non-cytotoxic materials
Cochis et al. [18]	<ul style="list-style-type: none"> • Paladon 65 – HR precoated with biosurfactant 	<ul style="list-style-type: none"> • MTT 	–	<ul style="list-style-type: none"> • L929 fibroblast cell line • human keratinocytes 	<ul style="list-style-type: none"> • surfactants on resin for prosthetic devices were non-cytotoxic

HR – heat-polymerized resin; PMMA – polymethylmethacrylate; AgNP – silver nanoparticles; AgNP – silver nanoparticles; AR – acrylic resin; POM – polyoxymethylene (acetal resin); R + NAC – N-acetyl cysteine supplemented resin (antioxidant); MMA – methyl methacrylate; SOD – superoxide dismutase; COL – collagen; *Gsta1* – glutathione S-transferase alpha 1 gene; MMA_r – residual methyl methacrylate concentration; MUPB – methacryloyloxyundecylpyridinium bromide (antiseptic); MMT – montmorillonite (nanocomposite); AuR – auto-polymerized resin; h – hours; d – days.

Polymerization Methods

According to Ebrahimi Saravi et al. [10], Tay et al. [5] and Ata & Yavuzylmaz [2], factors such as polymerization methods, temperature, the cycle of polymerization and acrylic resin storage time can influence the monomer quantity and the material cytotoxicity.

Based on the polymerization method, acrylic resin can be classified as heat-polymerized, microwave-polymerized, light-polymerized and auto-polymerized, the latter being the most common in dental practice [2, 6]. Its composition consists of a solid part of PMMA and a liquid part of MMA monomer [3, 6]. The low cost, the use at room temperature, the short process time and no additional equipment requirement for its manipulation are some of its advantages [11]. But, heat-polymerized resin is frequently used for denture base fabrication which maintains intimate contact with oral mucosa. Similarly, its composition is based on PMMA [8, 10].

When different polymerization methods are compared, auto-polymerized acrylic resin releases more residual monomers than heat-polymerized resin since the increase of temperature in the latter results in molecular chain movement which converts monomers into polymers [10]. Ebrahimi Saravi et al. [10] observed that auto-polymerized resin exhibited higher cytotoxicity level than heat-polymerized resin after 1 and 24 h of incubation. Similarly, Ata & Yavuzylmaz [2] reported significant higher cytotoxicity of auto-polymerized resin in a 24 h period. According to Ebrahimi Saravi et al. [10], lower levels were observed after 24 h because of the lower monomer levels in contact with cells. So, the cytotoxicity effect is dose-dependent.

Trubiani et al. [14] compared the cytotoxic effect of three polished and unpolished auto-polymerized acrylic resins. Cell growth reduction and an increase of pro-inflammatory cytokines were caused by the tested material, specially for unpolished resins. Therefore, the polishing procedure is important in clinical practice to reduce gingival inflammation.

Post-polymerization heat treatments, such as water bath or microwave irradiation, have been suggested in order to reduce the quantity of auto-polymerized acrylic resin residual monomers [5, 10, 11]. Bural et al. [11] affirmed that groups which were submitted to water immersion showed a reduction in MMA monomer formation when compared to untreated groups. Thus, water immersion is recommended. Similarly, Bural et al. [8] evaluated different polymerization cycles of heat-polymerized resins and observed an increase of

MMA residual monomers in specimens that were not immersed in water. Therefore, the longer the prosthesis is maintained in water media prior to its installation, the greater the monomer diffusion and less damage to the patients [5, 10].

However, Tay et al. [5] compared the cytotoxic effect of silicon-based soft liner, acrylic-based soft liner and tissue conditioner, and found that, despite the soft liner resins having shown slight to moderate cytotoxicity levels, heat-treatment did not reduce their cytotoxic effect. Kanie et al. [15] evaluated different soft lining materials based on urethane acrylate oligomers and observed that all of them showed high cell viability.

Acrylic Resin Cytotoxicity

Biocompatibility or cytotoxicity absence is defined by the material's ability to perform its function without inducing undesirable local or systemic effects [2].

Several substances such as N-Acetyl cysteine (NAC) [3, 6, 7], silver nanoparticles (AgNP) [1] and montmorillonite nanocomposite [13] were incorporated in the acrylic resin in order to evaluate their cytotoxic effects. Carbon-graphite fiber-reinforced composites (based on MMA/PMMA) [16] and associations between MMA and glycidyl methacrylate (GMA) with elemental iodine [17] were also evaluated for cytotoxicity. The authors observed biocompatibility of the tested substances.

Regis et al. [12] compared the cytotoxicity of the MMA monomer in relation to methacryloyloxyundecylpyridinium bromide (MUPB) and identified that, despite the fact that MUPB is more cytotoxic than MMA monomer, high concentrations of MMA reduces a cell's viability.

Cochis et al. [18] evaluated the influence of a precoating with biosurfactants that prevents *Candida albicans* biofilm formation on the cytotoxicity of acrylic resin for heat-polymerized denture base and silicon material. The biosurfactants on prosthetic materials were non-cytotoxic. Additionally, the authors observed that the biosurfactants reduced the biofilm activity.

Although Ata & Yavuzylmaz [2] affirmed that acrylic resin is a low biological risk material, several authors have reported signs and symptoms in patients as a result of its residual monomer exposure. Local chemical irritation [8, 9, 19], hypersensitivity, mucosal inflammation and ulceration [8, 9, 11], burning sensation in the palatal mucosa, tongue, oral mucosa and oropharynx, pain, edema, swelling and local erythema and labial edema [5, 9] and respiratory irritation [19] are reported clinical conditions.

Additionally, fibrosis, necrosis, histiocytosis [3, 6], inflammatory infiltrate and a thicker

keratin layer [5] were observed in the tissues in contact with the acrylic resin. Cytotoxicity has been reported in the literature as a result of exposure to unpolymerized resin components which cause genetic cell damage and oxidative stress [3, 6, 7].

Hattori et al. [4] studied the effect of MMA on mRNA expression of the glutathione S-transferase alpha 1 gene (*Gsta1*), presented in high amounts in hepatocytes, and observed that MMA increased *Gsta1* transcription. It is known that the liver is an organ related to detoxification. Therefore, MMA can induce cytotoxic effects in hepatocytes.

Changes in basic cell structure and function include the loss of membrane integrity, alteration of enzyme activities and synthesis of macromolecules [6], reduction of antioxidants [3, 6], cessation of cell growth, reduction of viability [7] and inhibition of cell proliferation and differentiation, gene mutation, delay of cell cycle, induction of cell apoptosis and necrosis [3, 6].

Acrylic resin cytotoxicity is associated, most times, with the presence of residual monomers

in the polymerization process. The monomers change cell morphology and function which can reduce their viability.

Since acrylic resins are widely used in dental practice, an adequate biocompatibility is essential. Considering that the majority of studies reported acrylic resin toxicity responses, further studies with different assessment methods are necessary for the development of biocompatible materials.

Final Considerations

There are different methods to evaluate acrylic resin cytotoxicity, with the MTT method being the most common test. In general, there is not a non-cytotoxic acrylic resin available on the dental market. Regarding the polymerization method, the auto-polymerized resin is more cytotoxic than heat-polymerized resin. The cytotoxic effect is dose dependent and depends on the amount of residual monomers. Residual monomers are responsible for inflammatory reactions of tissues in contact with the acrylic resin.

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